

# Hearing aid performance characterized by apparent SNR estimation to predict speech intelligibility in noise with hearing impaired listeners

Christophe Lesimple & Barbara Simon, Bernafon AG

## Interpreting changes in SRTn

Adaptive speech reception threshold in noise (SRTn) is one possible measurement used to evaluate and compare different hearing aids or algorithms. Interpreting changes in SRTn might be complex because:

- 1 performance of some tested features, algorithms or hearing aids is SNR dependent<sup>5,6</sup>,
- 2 differences between SRTn depend on the tested SNR range<sup>5,6</sup> which varies with the noise type, the speech material, the scoring method, speech and noise locations, and
- 3 SRTn changes represent a threshold shift of the psychometric function (PMF), but don't detect changes in slope or shape<sup>3,6</sup>.

In order to better understand SRTn changes, we propose to estimate the effect of two hearing aids, on output SNR and speech level, and model the experimental data from an adaptive SRTn over a broader SNR range<sup>6,8</sup>.

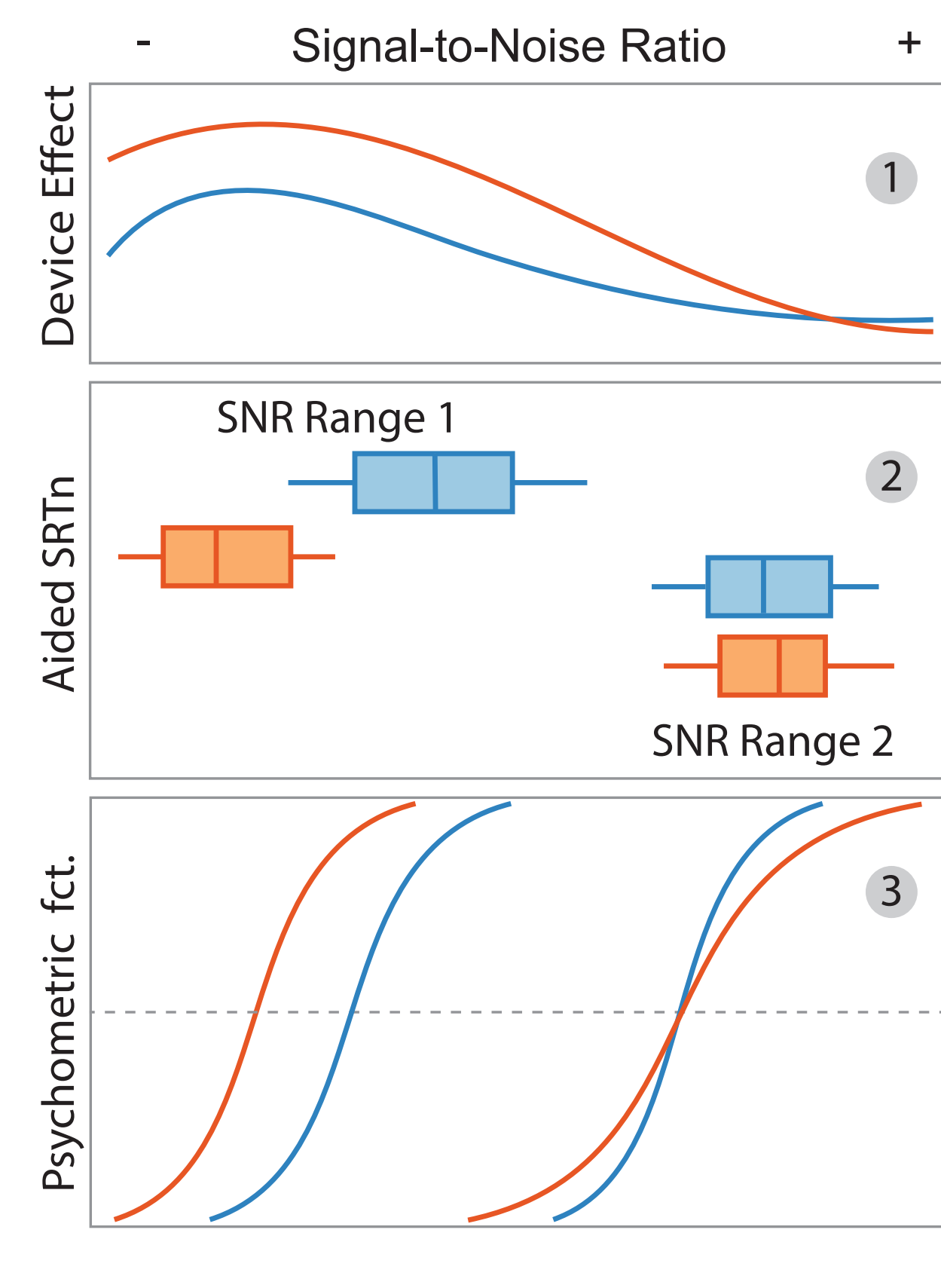
## 1 Device evaluation

Evaluation of 2 hearing aids (HA) with the same dynamic compression architecture. Directionality and noise reduction systems are different for the:

- **Reference HA** with pinna cue like directivity and modulation based noise reduction in 4 bands,
- **Test HA** with SNR optimized directivity and fast noise reduction in 16 bands.

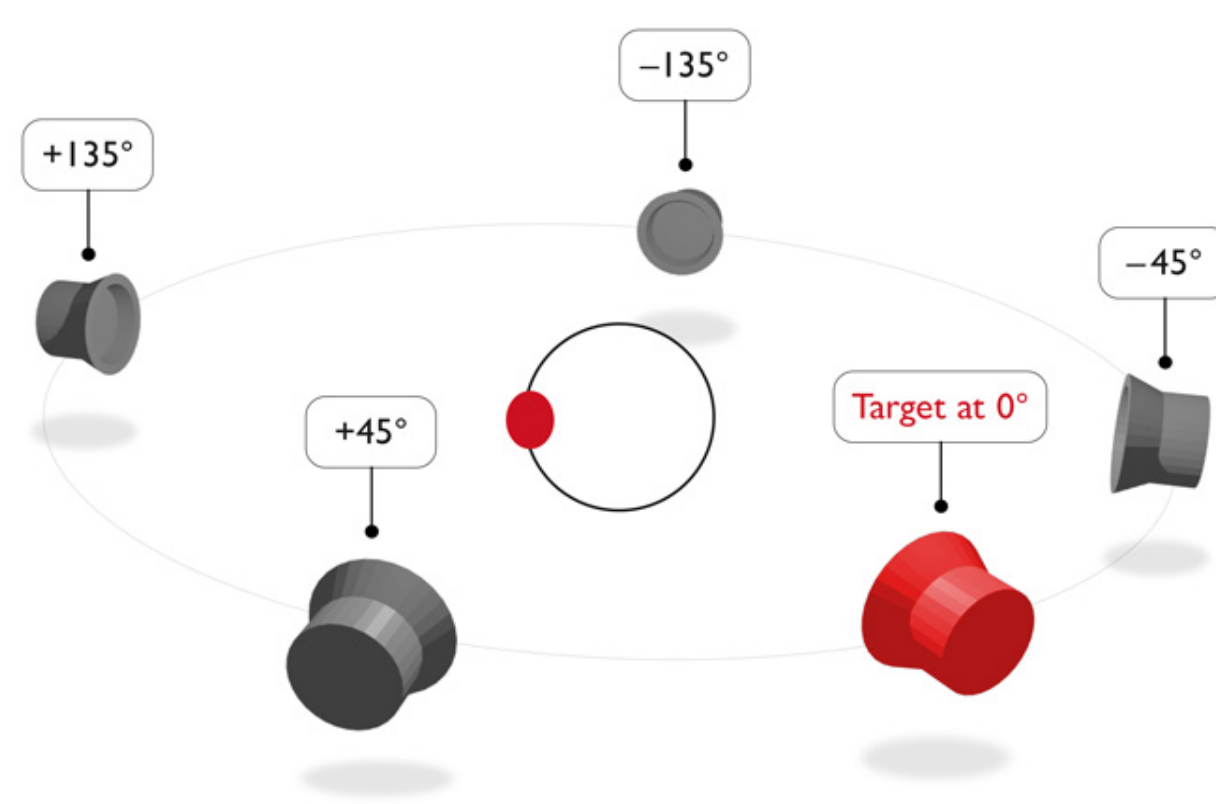
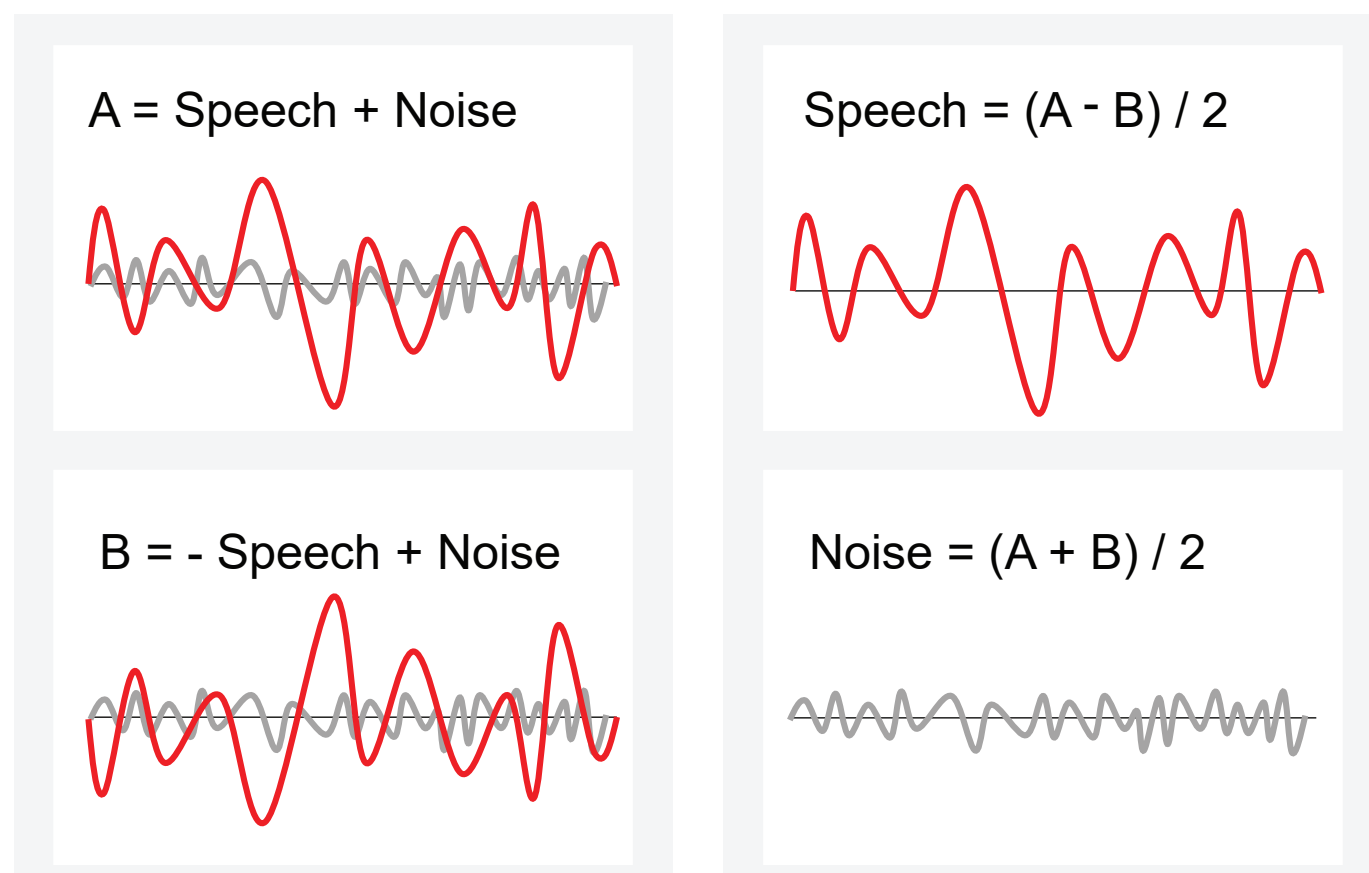
HA fitted with a N3 hearing loss<sup>1</sup>, NAL NL2 rationale and closed dome on KEMAR. Measured variables: HA output SNR and speech level.

HA evaluation with inversion technique<sup>2</sup> to separate two signals at the HA output: OLSA speech and noise from recording A and B. Fixed noise level at 65 dB SPL from  $\pm 45^\circ$  and  $\pm 135^\circ$  and speech from  $0^\circ$  [55-75 dB SPL].

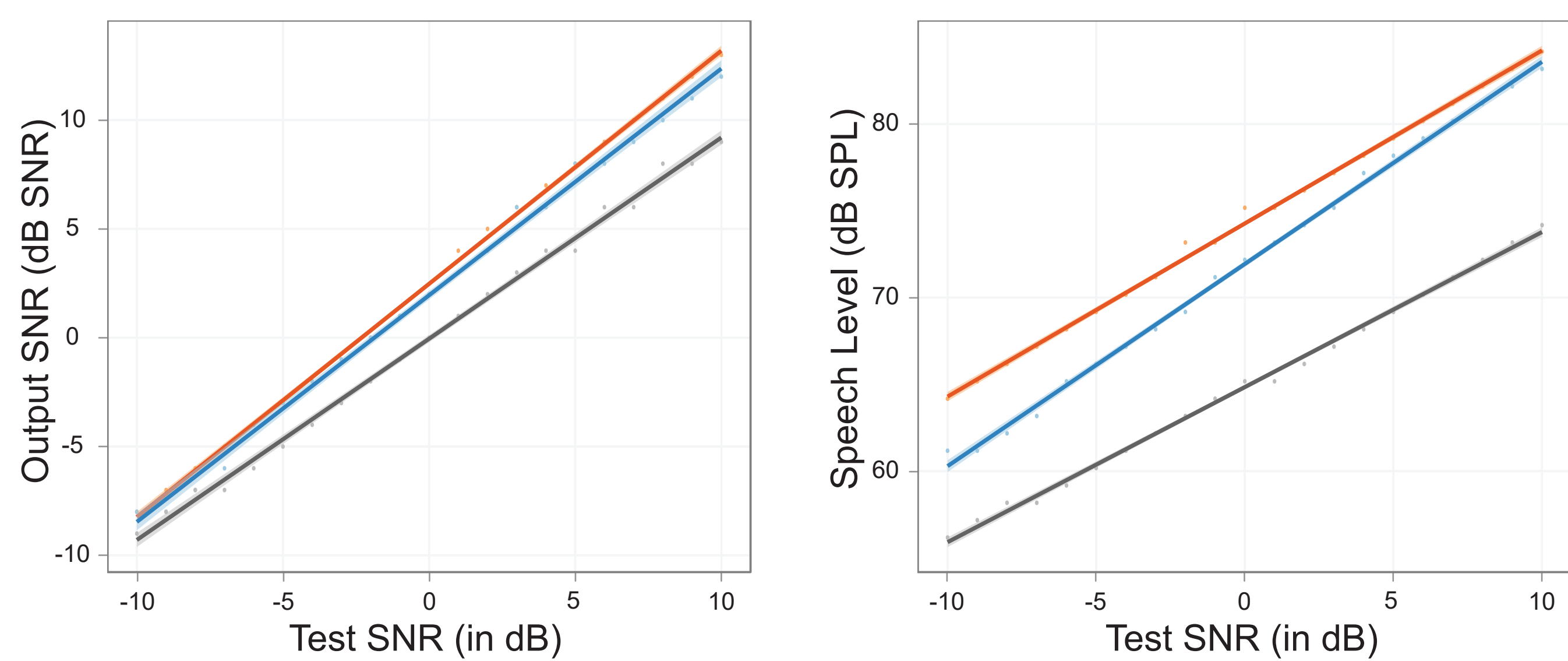


### Recording A and B

### Post-processing



— Unaided — Ref. HA — Test HA

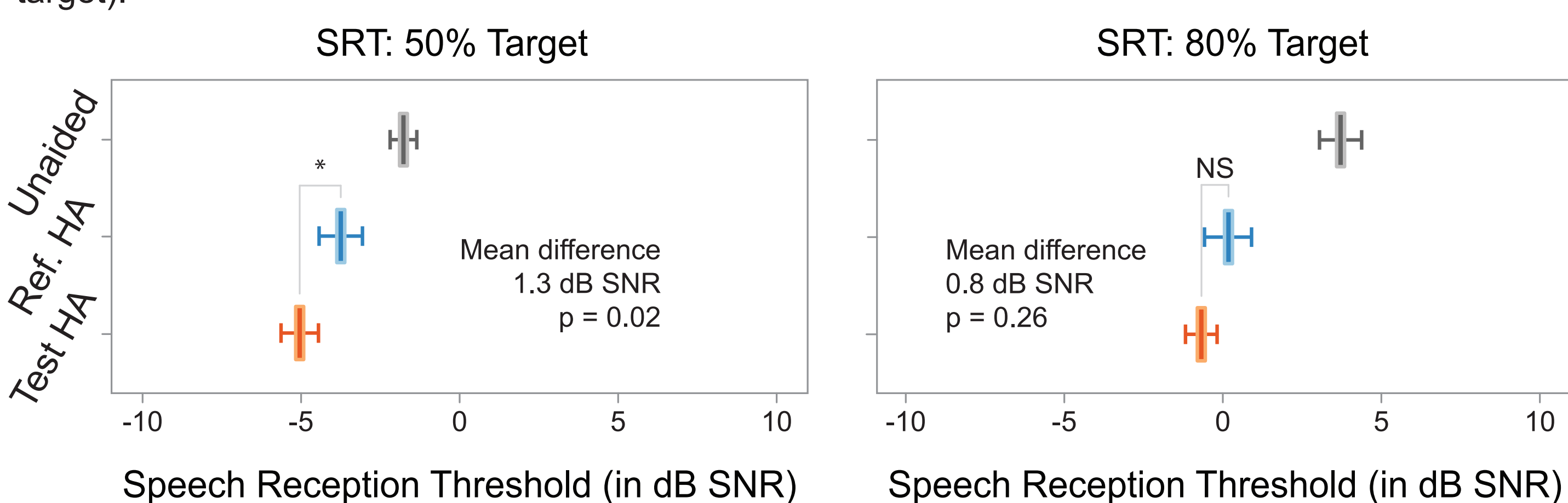


## 2 SRTn analysis

Subjects: 29 experienced hearing aid users, mild to severe hearing loss, HA gain based on NAL-NL2 rationale. Age range between 38 and 86 years old.

OLSA test: adaptive SRTn procedure targeting 50% and 80% intelligibility. Fixed noise at 65 dB SPL from  $\pm 45^\circ$  and  $\pm 135^\circ$  and adaptive speech from  $0^\circ$  starting at +5 dB SNR.

Differences between the reference and tested HAs depend on the SNR test range (changes with the % target).

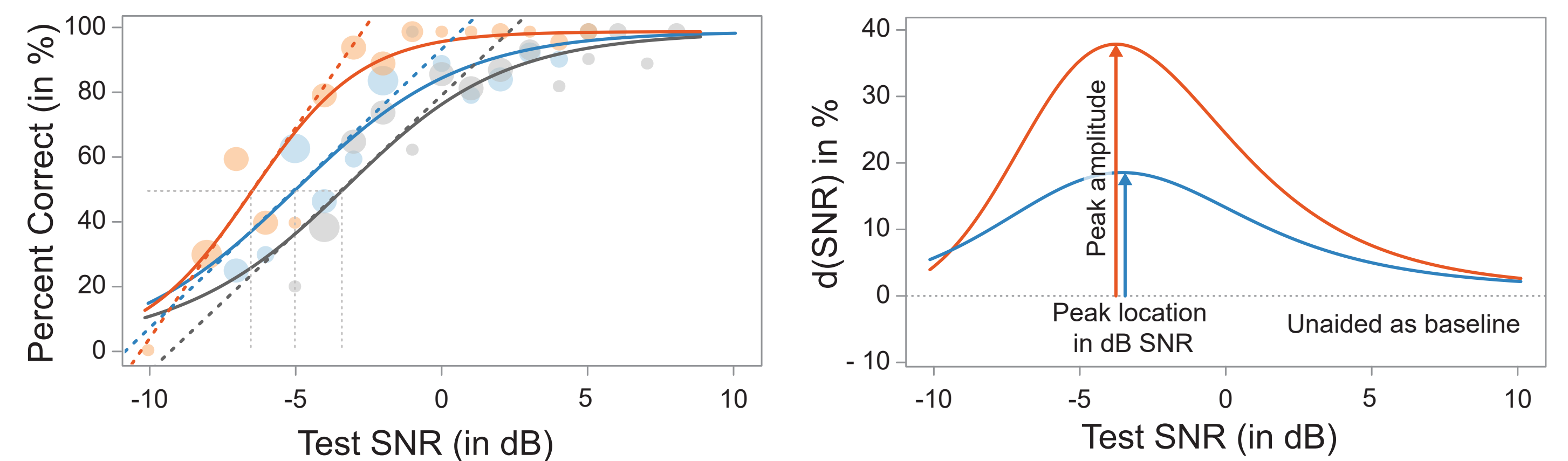


## 3 Individual d(SNR)

For each test subject, data are fitted over a broader SNR range based on a logistic distribution function with each tested condition<sup>4,8</sup>.

From the illustration, we observe that changing to the test HA, improved the SRT<sub>50</sub> but also increased the slope of the PMF.

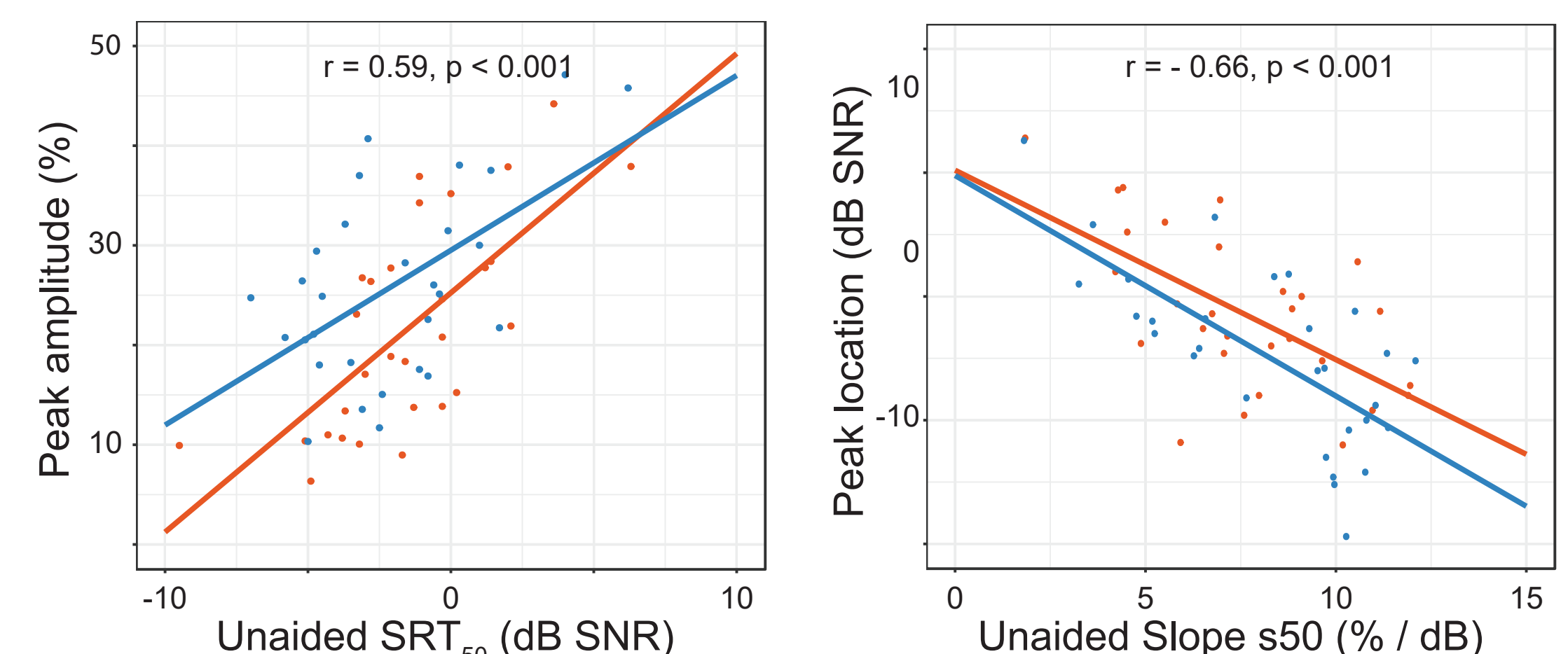
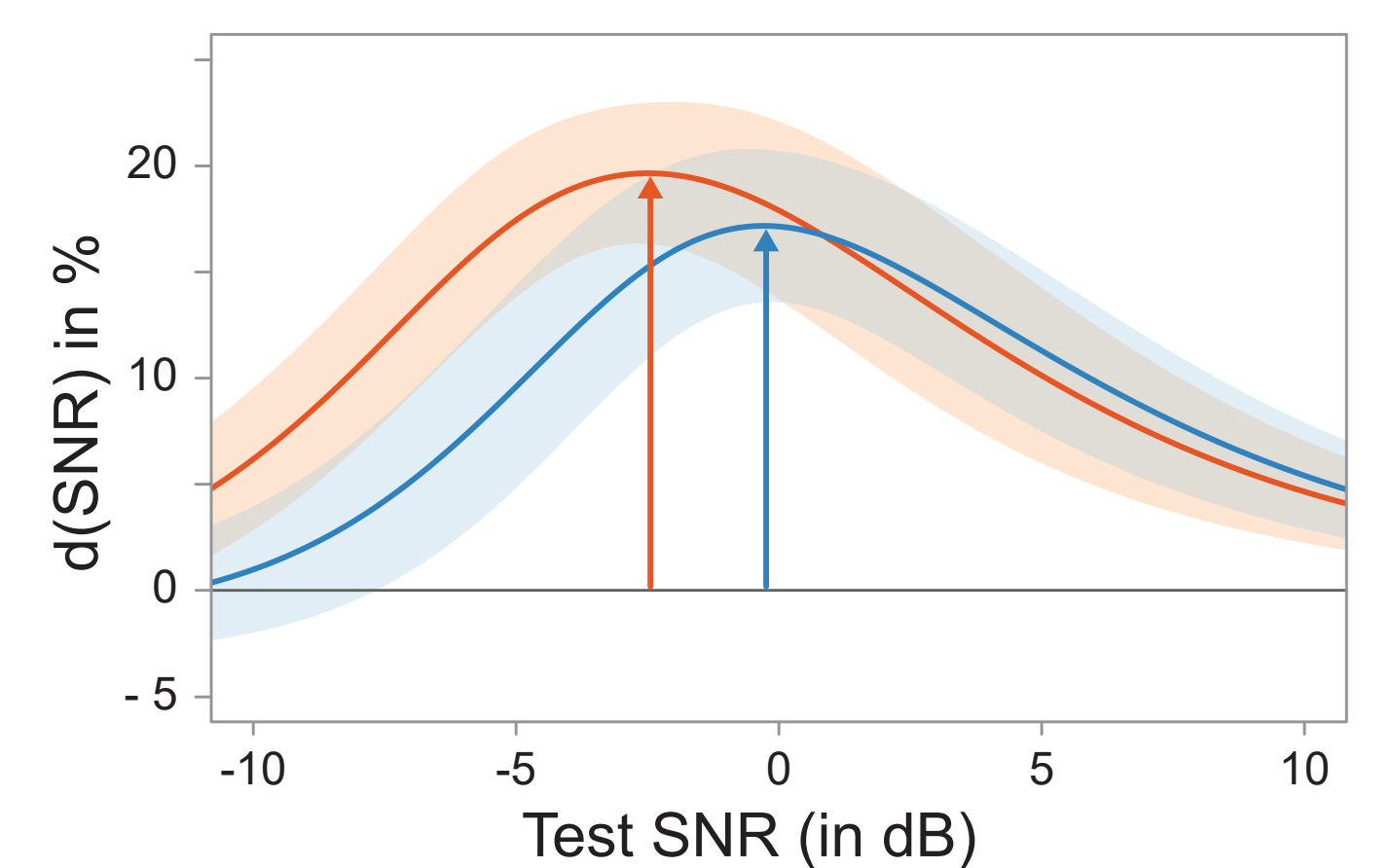
Difference between aided and unaided PMFs is expressed as the d(SNR)<sup>6</sup>. Peak location and amplitude are indicators to find the SNR that gives the maximum amplification benefit.



## Group d(SNR)

Averages and confidence intervals of d(SNR)s show 1) an overlap between both HAs for positive test SNRs (ceiling effect), and 2) a shift in peak location and an increase in peak amplitude with the tested HA at negative test SNRs.

Individual performances described by unaided SRT<sub>50</sub> and slope s50<sup>3</sup> are respectively associated with peak amplitude and peak location, i.e. individuals with more difficulties have larger peak amplitude and higher peak location. Benefit from amplification depends on individual characteristics.



## Predicting intelligibility changes

**Explanatory variables:** test subject (4 frequency pure tone average, age, unaided SRT<sub>50</sub>, and s50), test condition (device, changes in speech SPL and output SNR at the peak location). Subjects are included as random effect.

**Model selection:** backward stepwise selection<sup>7</sup>. 1) Removing influential observations based on Cook's distance. 2) Limiting collinearity with variation inflation factors below 2. 3) Testing models without low contributing fixed effect based on likelihood ratio test.

### Peak location:

- the test device will shift the peak by -1.4 dB SNR,
- is lower for listeners with low unaided SRT and steep unaided slopes.

### Peak amplitude:

- is increase by 5% with the test device,
- is higher for listeners with high unaided SRT and steep unaided slopes.

Unaided SRT and slopes have different effects in peak location and amplitude.

Effect	Estimate	SE	t.value	p
device	-1.42	0.38	-3.71	< 0.001
delta.SNR	1.77	0.66	2.65	0.01
unaided SRT <sub>50</sub>	0.37	0.11	3.34	0.002
unaided s50	-67.8	10.7	-6.34	< 0.001
age	-0.02	0.03	-0.64	0.53

Effect	Estimate	SE	t.value	p
device	0.05	0.13	0.85	0.04
delta.SNR	0.01	0.03	0.41	0.69
unaided SRT <sub>50</sub>	0.02	0.004	4.36	< 0.001
unaided s50	0.85	0.44	1.94	0.06
PTA	0.002	0.002	1.29	0.21
age	-0.001	0.001	-0.77	0.45

## Discussion

- Differences in SRTn between test conditions depend on the SNR range and on listeners' characteristics. Modelling the PMF and measuring device performance over a broader SNR range should help to evaluate the differences between test conditions.
- The SNR range where the test HA reduces the target loss corresponds to the SNR range where the differences in intelligibility are maximized.
- A significant difference or an absence of changes in traditional SRTn are not enough to generalize the findings. Reality might be more complex.

Contact: cles@bernafon.com

Both devices are commercially available: **Juna 9** for the reference and **Zerena 9** for the tested device.

## References

- 1) Bisgaard, N., Vliaming, M. S. M. G., & Dahlquist, M. (2010). Standard Audiograms for the IEC 60118-15 Measurement Procedure. Trends in Amplification, 14(2), 113-120.
- 2) Hagerman, B., & Olofsson, A. (2004). A Method to Measure the Effect of Noise Reduction Algorithms Using Simultaneous Speech and Noise. Acta Acustica, 90, 356-361.
- 3) Hey, M., Hocke, T., Hedderich, J., & Müller-Deile, J. (2014). Investigation of a matrix sentence test in noise: Reproducibility and discrimination function in cochlear implant patients. International Journal of Audiology, 53(12), 895-902.
- 4) Kno-blauch, K., & Maloney, L. T. (2012). Modeling Psychophysical Data in R. Springer NY.
- 5) Naylor, G. (2016). Theoretical Issues of Validity in the Measurement of Aided Speech Reception Threshold in Noise for Comparing Nonlinear Hearing Aid Systems. Journal of the American Academy of Audiology, 27(7), 504-514.
- 6) Rhebergen, K. S., Maalderink, T. H., & Dreschler, W. A. (2016). Characterizing Speech Intelligibility in Noise After Wide Dynamic Range Compression. Ear and Hearing, 1, 7.
- 7) Zuur, A. F., Ieno, E. N., & Elphick, C. S. (2010). A protocol for data exploration to avoid common statistical problems. Methods in Ecology and Evolution, 1(1), 3-14.
- 8) Zychaluk, K., & Foster, D. H. (2009). Model-free estimation of the psychometric function. Attention, Perception, and Psychophysics, 71(6), 1414-1425.